

Inclusion of Thermal Dependent Material Relations for Modeling Microwave Ablation Antennas

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Outline

1. What is Microwave Ablation?
2. Motivation
3. Antenna and model in QW
4. Results
5. Conclusion, what's next?



Microwave Ablation (MWA)

- Cancer treatment that uses microwave energy to generate heat
- Typically 900 MHz or 2.45 GHz
- Heating caused by friction of oscillating water molecules
- Cancer **tissues** are more likely to heat (more water molecules, higher conductivity)
- Modified coaxial cable is the simplest example of the MWA antenna
- Ablation Zone $\geq 60^{\circ}\text{C}$ **[4]**

References

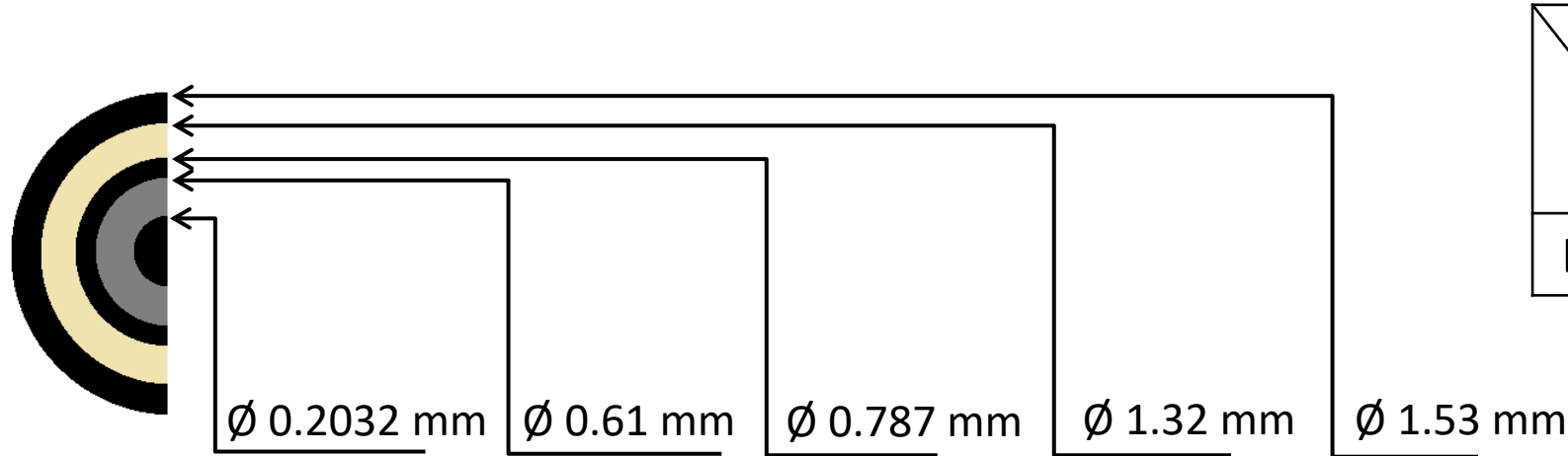
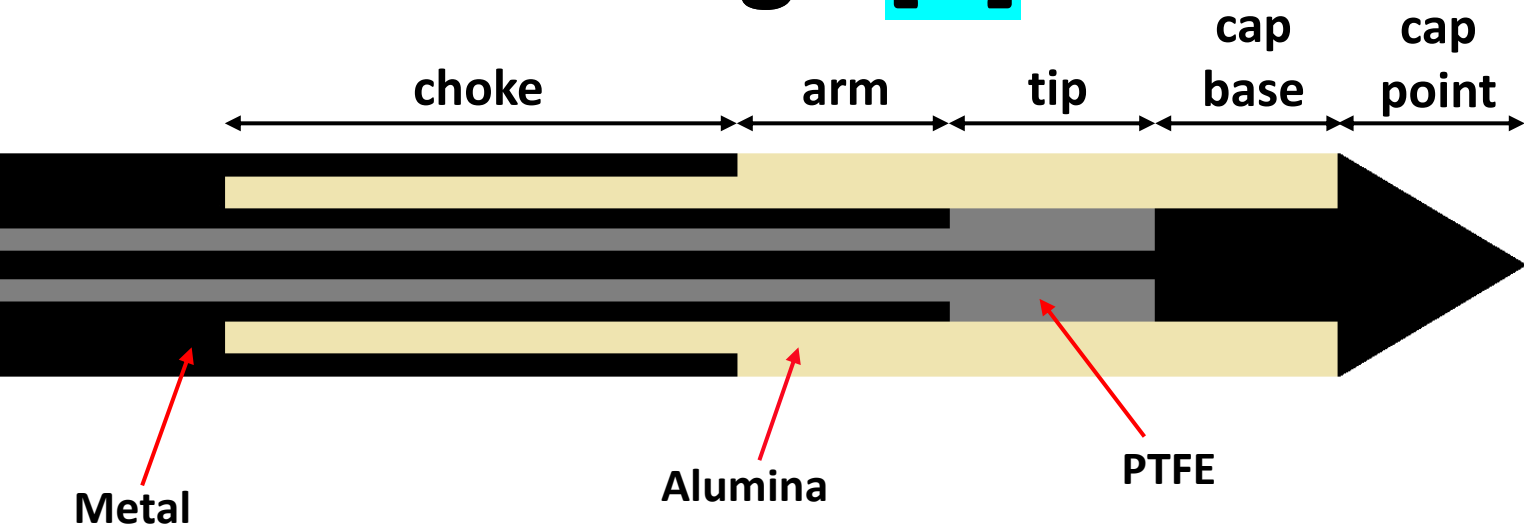
- [1] QWED, *QuickWave Basic Heating Module*. [Online] Available: https://www.qwed.com.pl/qw_bhm.html
- [2] M. Cavagnaro, C. Amabile, P. Bernardi, S. Pisa, and N. Tosoratti, “A Minimally Invasive Antenna for Microwave Ablation Therapies: Design, Performances, and Experimental Assessment,” *IEEE Transactions on Biomedical Engineering*, vol. 58, no. 4. Institute of Electrical and Electronics Engineers (IEEE), pp. 949–959, Apr. 2011. doi: 10.1109/tbme.2010.2099657
- [3] QWED (2023), *NanoBat – Coupled GHz Thermal workflow for a battery model*. [Online] Available: https://www.qwed.com.pl/nanobat_coupled_ghz_thermal_woorkflow.html
- [4] V. Lopresto, R. Pinto, L. Farina, and M. Cavagnaro, “Microwave thermal ablation: Effects of tissue properties variations on predictive models for treatment planning,” *Medical Engineering & Physics*, vol. 46. Elsevier BV, pp. 63–70, Aug. 2017. doi: 10.1016/j.medengphy.2017.06.008.



Motivation and Background

- Accurate simulations of microwave ablation antennas are essential for optimizing their design, predicting thermal distribution and improving clinical outcomes.
- We want to test and show capabilities of QuickWave FDTD simulator in simulating the MWA and further improve it.
- As a benchmark, we shall use designs and additional material parameters from paper [2].

Antenna Design [2]



| Medium | PTFE | Alumina |
|--------------|------|---------|
| Permittivity | 2.2 | 10 |

| Choke | Arm | Tip | Cap Base | Cap Point |
|-------|------|------|----------|-----------|
| 10 mm | 6 mm | 1 mm | 5 mm | 5 mm |

| | ϵ_r | σ (S/m) | ρ (kg/m ³) | C (J/kg·°C) | K (J/s·m·°C) |
|-------|--------------|-------------------|--------------------------------|----------------|-----------------|
| Liver | 43.03 | 1.69 | 1041 | 3600 | 0.51 |

Antenna Model in QW

BOR V2D

Cell size: $dx = 0.5 \text{ mm}$
 $dy = 0.1 \text{ mm}$

Number of cells with boundaries: 136144

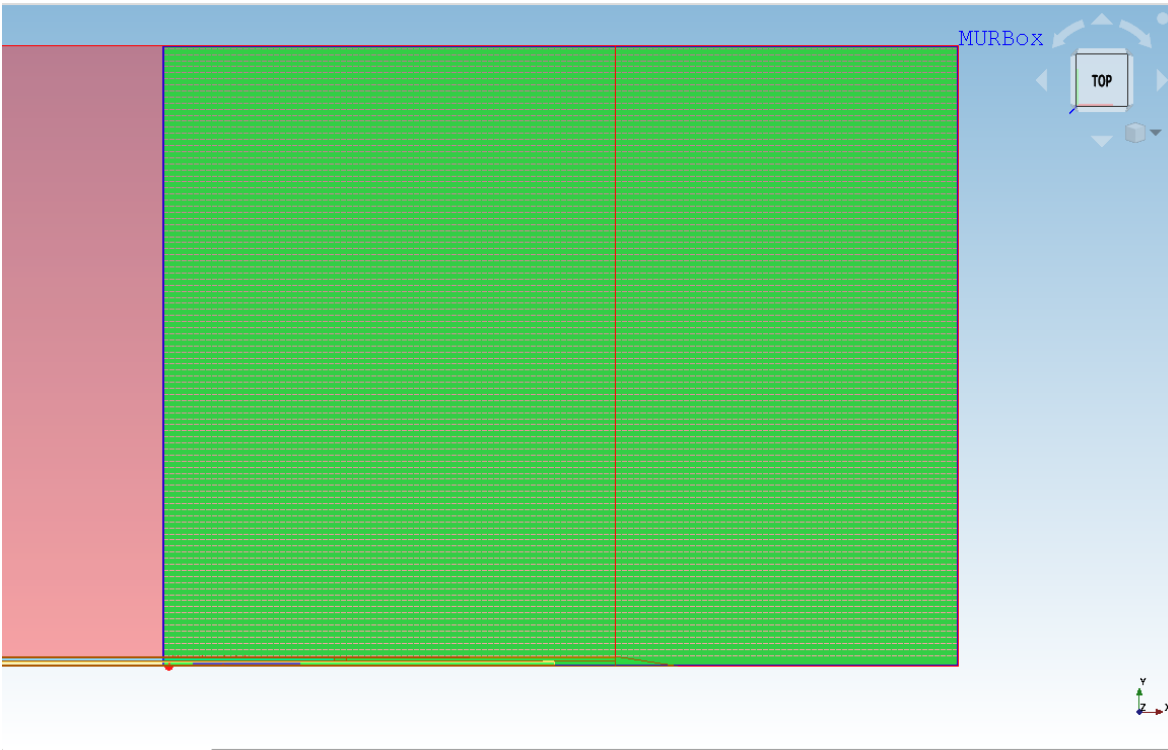
Project size (RAM): ~13 MB

Whole model size: 80 mm x 50 mm

Length of the antenna: 57 mm

TEM field at 2.45 GHz

Heating: 15 min – 20 W



Antenna Model in QW

The QW-BHM is a heating module that was used in several projects before [1, 3].

The three different setups were applied:

- Neumann Boundary Condition without heatflow
- Neumann Boundary Condition with heatflow
- Neumann Boundary Condition with heatflow and temperature-dependent liver parameters

Antenna Model in QW

Temperature-Dependent parameters of the liver

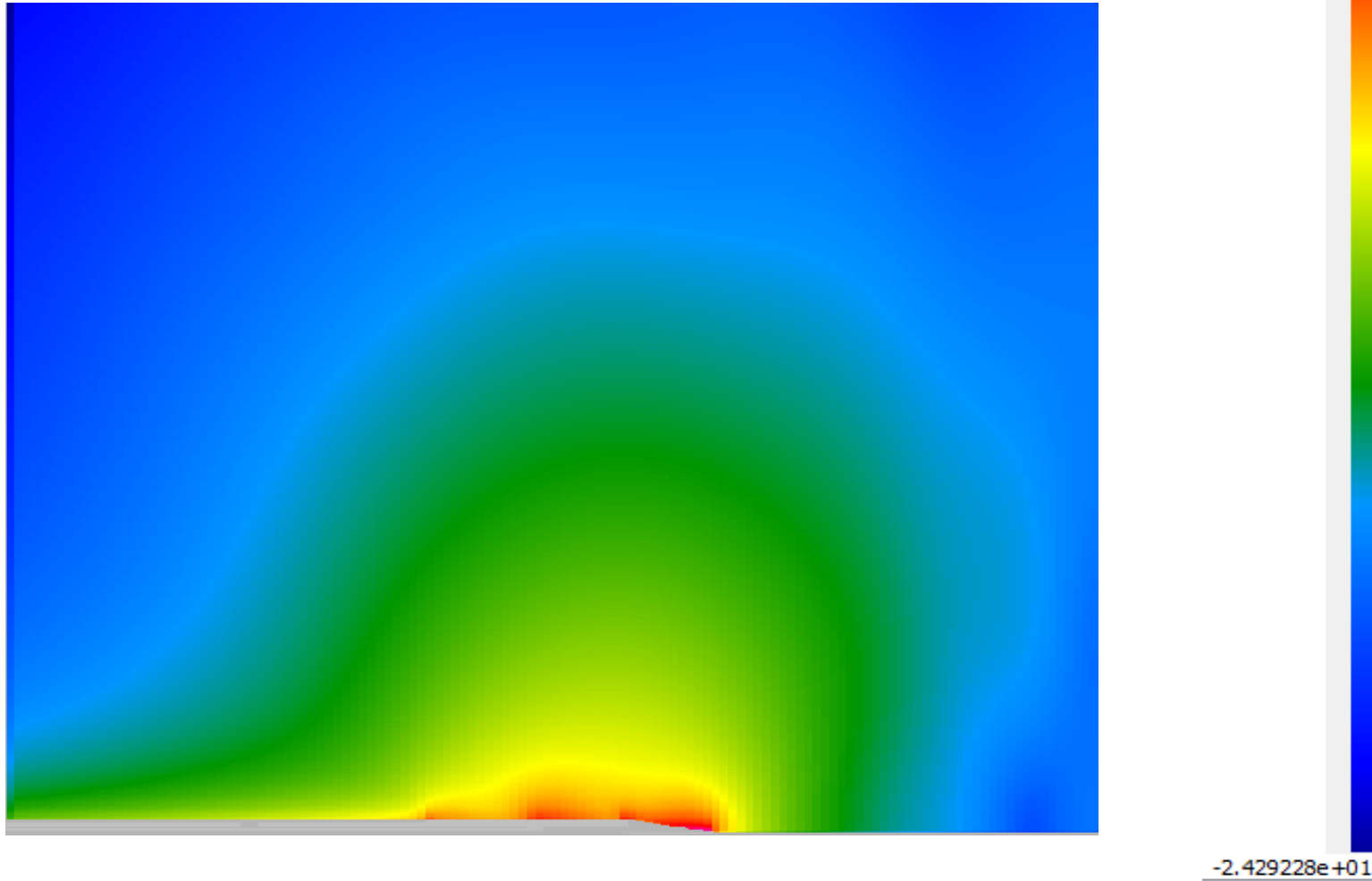
DATA FROM -20 C to +80 C, dH/dV in J/cm3 reversedEnth/Temp column

| !Temperature | Enthalpy | EPa | SIGa | SpecHeat | Density | Ka |
|--------------|----------|------|-------|----------|---------|--------|
| # Data deg C | J/cm3 | | S/m | | | |
| -20 | 0 | 4.9 | 0.064 | 2.21 | 1.041 | 0.0051 |
| -15 | 14.0 | 5.5 | 0.093 | 2.21 | 1.041 | 0.0051 |
| -10 | 34.4 | 6.1 | 0.153 | 2.21 | 1.041 | 0.0051 |
| -5 | 71.4 | 12.3 | 0.573 | 2.21 | 1.041 | 0.0051 |
| -3 | 110.4 | 22.0 | 1.118 | 2.21 | 1.041 | 0.0051 |
| -2.2 | 144.4 | 30 | 1.636 | 2.21 | 1.041 | 0.0051 |
| -1.6 | 192.4 | 42 | 2.113 | 2.21 | 1.041 | 0.0051 |
| -1.3 | 240.4 | 46 | 2.385 | 2.21 | 1.041 | 0.0051 |
| -1.1 | 274.4 | 48.9 | 2.426 | 2.21 | 1.041 | 0.0051 |
| -1.0 | 288.4 | 49.2 | 2.440 | 2.21 | 1.041 | 0.0051 |
| 10 | 327.9 | 48.9 | 2.317 | 2.21 | 1.041 | 0.0051 |
| 20 | 382.9 | 48.2 | 2.194 | 2.21 | 1.041 | 0.0051 |
| 35 | 450.4 | 46.9 | 2.072 | 2.21 | 1.041 | 0.0051 |
| 50 | 517.9 | 45.5 | 1.949 | 2.21 | 1.041 | 0.0051 |
| 65 | 585.4 | 43.6 | 1.922 | 2.21 | 1.041 | 0.0051 |
| 80 | 652.9 | 41.7 | 1.908 | 2.21 | 1.041 | 0.0051 |

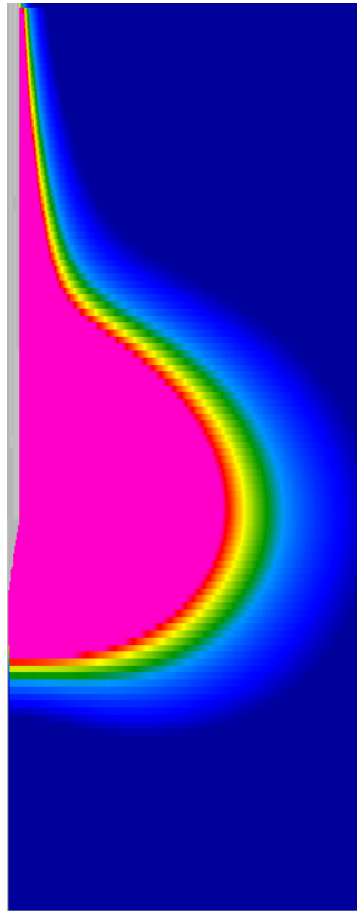
Each values of the parameters are defined for each value of the temperature

Measurements & refinements by Per O Risman, Microtrans AB, Sweden

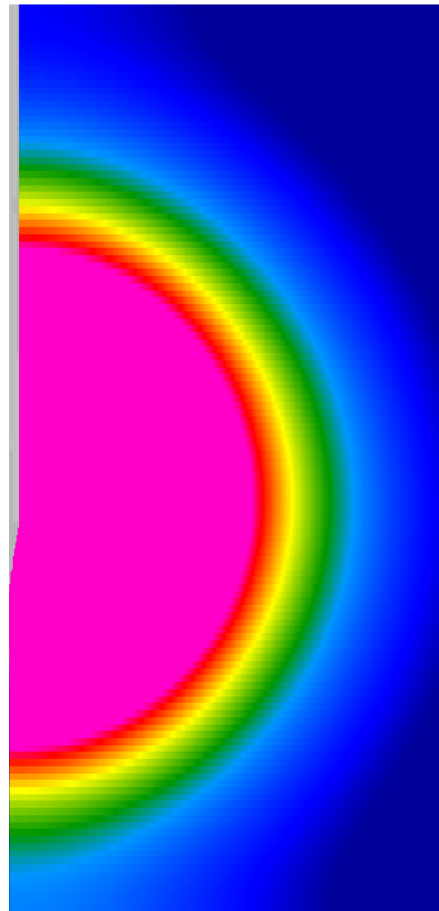
Results -Average SAR Distributions



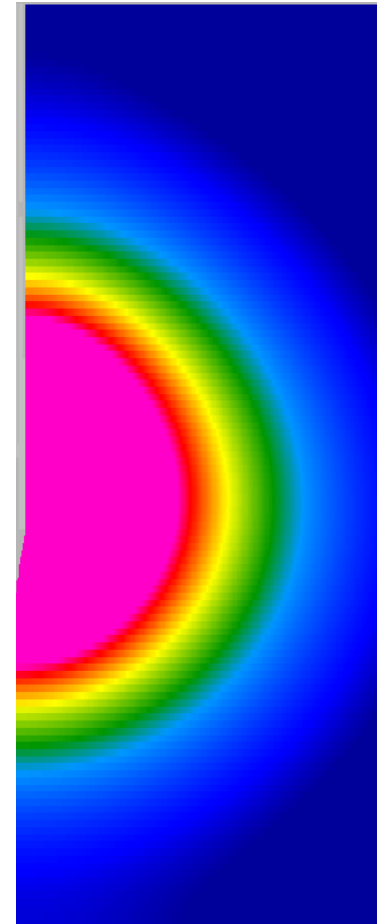
Results - Ablation Zones



NBC w/o HF



NBC with HF



NBC with HF
and TD
parameters



The maximum is
set to 60°C so
the ablation
zones can be
clearly visible

Results - Ablation Zones

Ablation Zones Dimensions.

| | Length x Diameter (mm) |
|--|---------------------------|
| Experiment | 38 x 31 |
| NBC+HF | 36 x 35.48 |
| NBC | — x 31.28 |
| NBC+HF+TD material parameters | 25 x 23.08 |

Using the heat distribution, ablation zones ($\geq 60^{\circ}\text{C}$) were determined.

In that case it is impossible to determine the length of the AZ cause to its irregular shape.



Conclusions

- The difference between the results may have several reasons like inaccurate experimental methods and due to differences in the parameters of the real liver and those assumed in the model
- Adding the bio-heat equation to BHM should make the results more precise
- Further works requires an experimental method that will allow for more precise determination of the ablation zone and parameters of the liver or other samples



We are open to new collaborations!

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